



**Pharmacy** 

Fused deposition modelling for the development of antiplatelet materials for cardiovascular applications



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School of

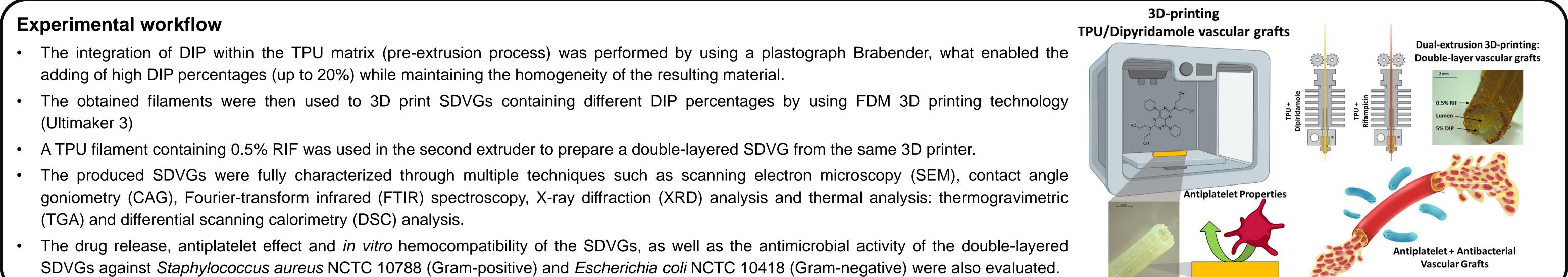
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## Abstract

This work describes the use of fused deposition modelling (FDM) to prepare antiplatelet thermoplastic polyurethane (TPU)-based small diameter vascular grafts (SDVGs). FDM 3D printing technology is widely available and provides the ability to easily design SDVGs on demand, enabling to customize the dimensions of the vascular prosthesis. An antiplatelet drug, dipyridamole (DIP), was combined with TPU using hotmelt extrusion to prepare filaments. DIP cargos ranged between 5 and 20% (w/w). The resulting filaments were used to prepare SDVGs using FDM. These grafts were physicochemically characterised and their performance was evaluated by testing DIP release kinetics, antiplatelet activity and the *in vitro* hemocompatibility. The results suggested these grafts were capable of providing a sustained DIP release for 30 days. Moreover, the resulting grafts loaded with 5% DIP showed a clear antiplatelet effect as opposed to grafts containing higher DIP cargos. The latter was related to sample surface roughness and hydrophilicity/hydrophobicity, as well as the drug loadings. Finally, DIP loaded TPU to prepare double-layered SDVGs. These grafts showed a clear antimicrobial activity against Staphylococcus aureus and Escherichia coli.



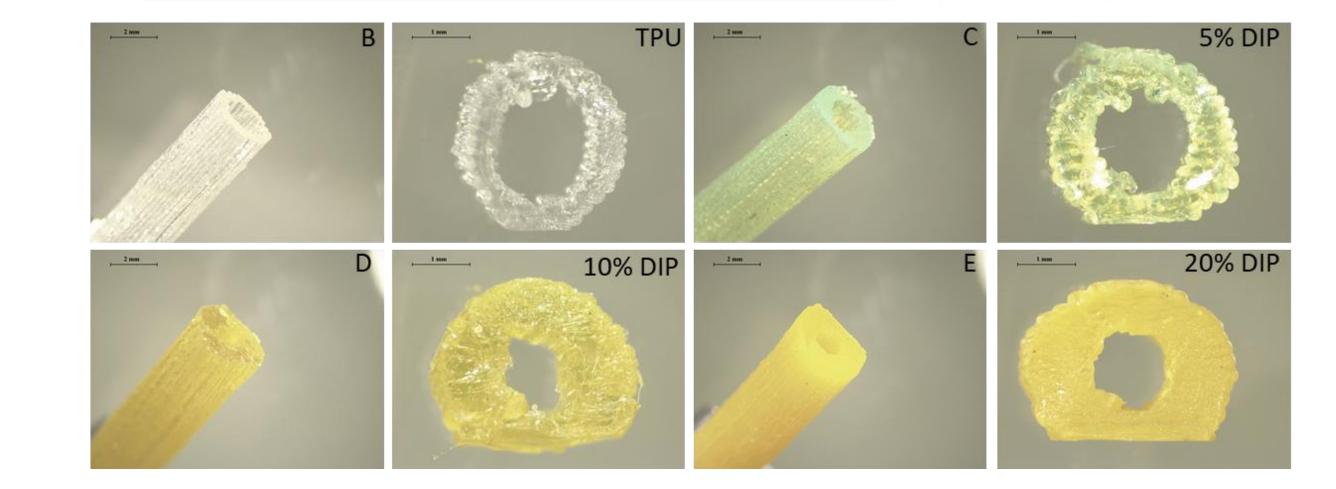
Wн

LH

## Results

#### **1. Preparation of DIP-eluting SDVGs**

A	3D printed model distance (mm)			
	L <sub>v</sub>	L <sub>H</sub>	W <sub>v</sub>	W <sub>H</sub>
CAD Model	2	2	0.5	0.5
TPU	$2.13 \pm 0.13$	$1.69 \pm 0.08$	$0.50 \pm 0.08$	$0.59 \pm 0.05$
5% DIP	$1.90 \pm 0.07$	$1.67 \pm 0.14$	$0.52 \pm 0.10$	$0.77 \pm 0.06$
10% DIP	$1.45 \pm 0.11$	$1.55 \pm 0.07$	$0.65 \pm 0.20$	$0.92 \pm 0.13$
20% DIP	$0.95 \pm 0.15$	$1.20 \pm 0.10$	$0.88 \pm 0.29$	$1.23 \pm 0.08$



# 2. SEM images of DIP-eluting SDVGs

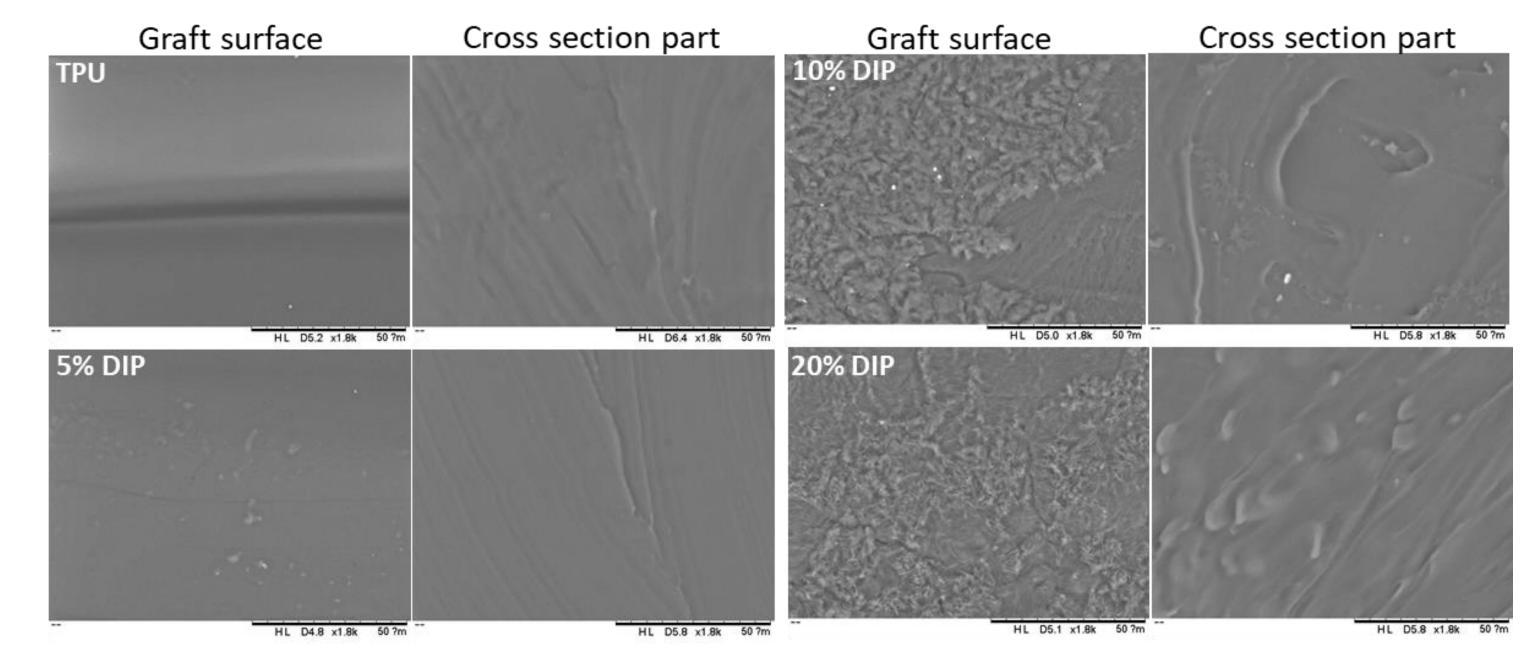


Figure 2: SEM images of the 3D-printed SDVGs surfaces containing different DIP concentrations and their cross sections. The SEM images showed that 3D-printed SDVGs containing no DIP and 5% DIP presented

Figure 1: Table showing the dimension of the 3D-printed SDVGs and the cross-section diagram of them with legend for these dimensions ( $n \ge 4$ ) (A). Light microscope images of the 3D-printed SDVGs and their cross-sections (B-E). SDVGs containing 5% DIP presented small differences when compared with the original computer-aided design (CAD) file

#### TPU 80 5% DIP <u>ة</u> 70 10% DIP angle 0 20% DIP 10% DIP 20% DIP 50 DIP 40 20 10 15 25 2600 2100 1600 1100 3600 3100 DIP content (%) Wavenumber (cm<sup>-1</sup>) — TPU ——5% DIP DIP 100 -20% DIP TPU 80 5% DIP 10% DIP 20% DIP — 5% DIP -10% DIP -20% DIP DIP powde 200 2 theta scale (2 $\theta$ ) Temperature (°C) Temperature (°C)

Figure 3: Influence of the DIP content on the contact angle of water with the DIP-loaded 3D-printed samples (n = 4) (A). FTIR spectra (B), XRD diffractograms (C) and TGA (D) and DSC curves (E) of each of the DIP-loaded 3D-printed samples. The contact angle measurements reported an increase in the surface hydrophilicity of the 3D printed scaffolds after increasing the DIP loadings (10% and 20%).

smoother surfaces in comparison with the SDVGs prepared with higher concentrations of DIP, which is ultimately influencing on the platelet adhesion.

#### 4. *In vitro* drug release

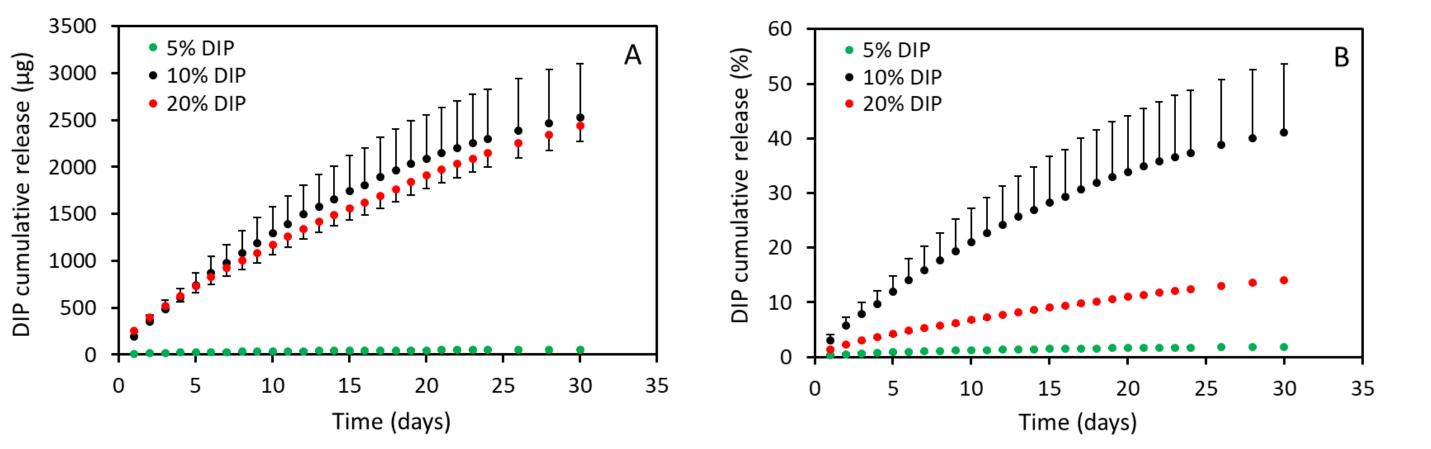
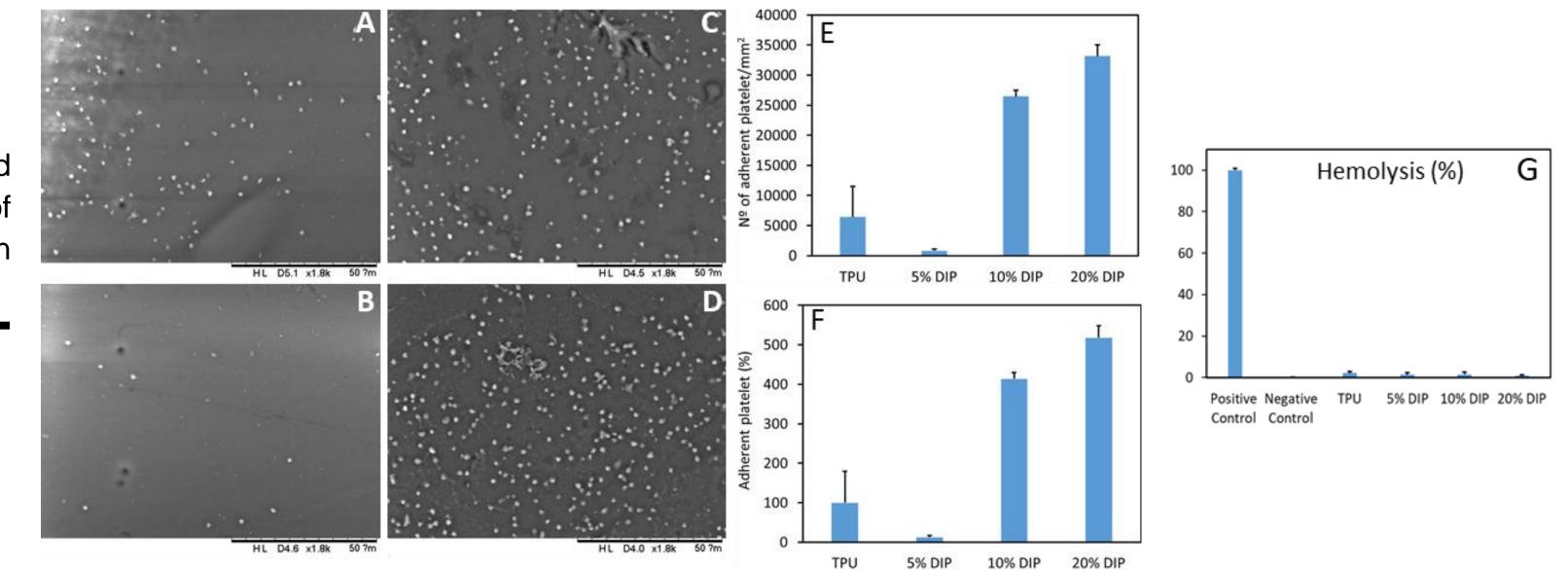


Figure 4: In vitro DIP release curves from DIP-eluting 3D-printed SDVGs up to 30 days in PBS at 37°C expressed in µg as function of time (A) and expressed in percentage as a function of initial DIP drug loading (B) (n = 4). DIP-eluting SDVGs showed a sustained drug release for 30 days and no obvious burst release was observed within the first 24 h.

## 5. Platelet adhesion and hemocompatibility of SDVGs



## 3. Physicochemical characterisation DIP-eluting SDVGs

## 6. Antimicrobial properties of the double-layered SDVGs

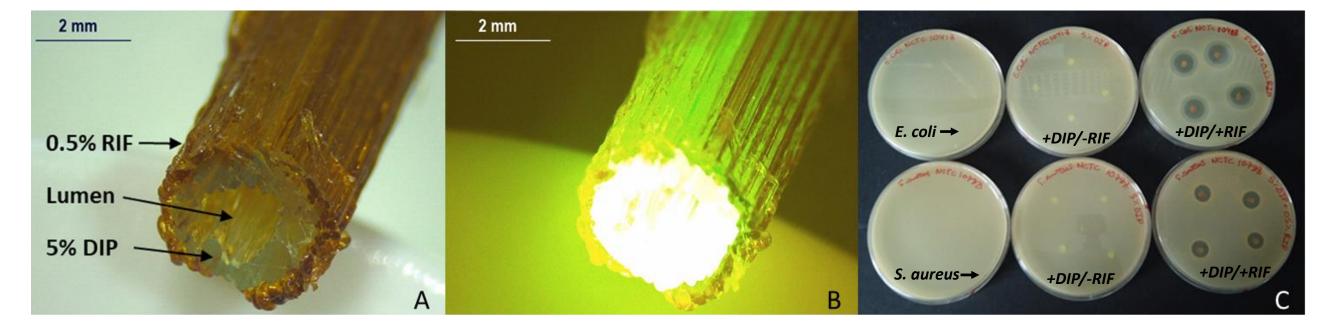


Figure 6: Light microscope image of a double-layered SDVG (A) and the same image using the NIGHTSEA Model SFA Stereomicroscope Fluorescence Adapter (B). A picture showing the zones of inhibition obtained for S. aureus and E. coli in MH agar using slices of the double-layered SDVG (C).

Figure 5: SEM images of rabbit blood platelet depositions on the surfaces of TPU (A), 5% DIP (B), 10% DIP (C) and 20% DIP-loaded 3D-printed samples (D). Results of the platelet adhesion study expressed in platelet/mm<sup>2</sup> (E), and expressed in percentage of platelets adhered to the samples surface, using TPU as reference (F). Rabbit blood hemolysis percentages of the DIP-loaded 3D-printed samples (G) (n = 5). This experiment showed that 5% DIP-loaded samples presented a clear antiplatelet effect. These results, therefore, highlights the importance of the DIP loading into the material.

#### Conclusions

- The characterisation of the resulting SDVGs suggested that after the extrusion and printing process the drug present in the samples was in an amorphous state. Moreover, 3D-printed SDVGs using filaments loaded with up to 5% (DIP) presented small differences when compared with the original CAD file.
- The results suggested that samples loaded with 5% DIP presented the highest antiplatelet activity. This can be due to its smoother and more hydrophobic surface. Therefore, these results are confirming the influence on the platelet adhesion of the surface roughness and hydrophilicity of the performed 3D-printed materials. Furthermore, all the 3D-printed samples prepared in this work were hemocompatible.
- A double-layered SDVG containing two different drugs DIP and RIF was also prepared and exhibited a clear antimicrobial activity against S. aureus and E. coli, pathogens involved in hospital-acquired infections (HAI)