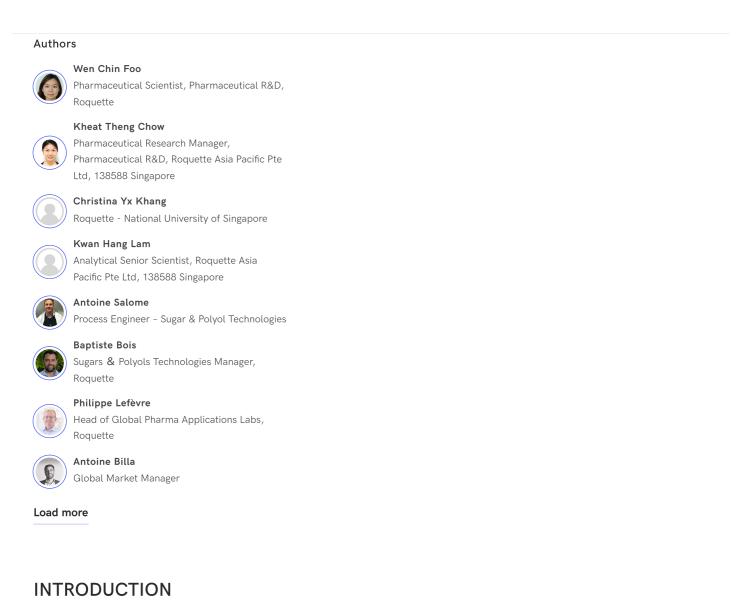


# Co-processed Hydroxypropyl Methylcellulose–Mannitol as a Directly Compressible Excipient for Controlled Release

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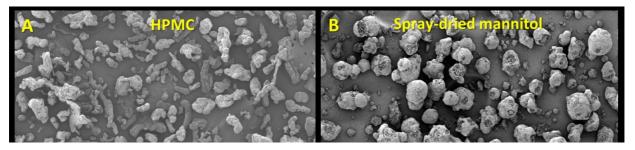
Controlled release dosage forms deliver an effective dose of the active pharmaceutical ingredient over a prolonged duration, which is particularly advantageous to maintain a constant plasma drug concentration within the therapeutic window. This effectively overcomes the negative peak-trough effects associated with multiple dosing of immediate release formulations. In addition, controlled release formulations also feature significantly in patient-centric pharmaceutical design, given the reduced administration frequency hence improved patient compliance. The most common strategy involves dispersing the active ingredient homogeneously in a hydrophilic polymer matrix, which hydrates and swells upon contact with biological fluids to form a viscous diffusion gel barrier which limits drug release. Hydroxypropyl methylcellulose (HPMC) is among the most widely used excipients as a water-soluble, hydrophilic controlled release matrix. However, standard HPMC powders are associated with flow issues due to their fibrous nature, rendering it unsuitable for tableting via direct compression. In this work, PEARLITOL® CR-H HPMC co-processed with mannitol from Roquette Frères was evaluated based on critical quality attributes necessary for a directly compressible, controlled release excipient. In addition to

## MATERIALS AND METHODS

Co-processed HPMC-mannitol was produced by spray-drying whereby HPMC particles were spray coated with mannitol solution. Particle morphology was assessed via scanning electron microscopy of powder samples sputter-coated with platinum. Moisture content was determined by loss on drying using a moisture analyzer (Ohaus<sup>®</sup> MB 45, USA). The flow properties of co-processed HPMC-mannitol (PEARLITOL<sup>®</sup> CR-H) were characterized via angle of repose, bulk/tapped density and flow through a 10 mm orifice measurements (Ph. Eur. Chapter 2.9.16), in comparison to direct compression grade HPMC (METHOCEL<sup>™</sup> DC2 K4M, Colorcon, USA) and physical mixtures of HPMC-mannitol. The mannitol used in the physical mixture was PEARLITOL<sup>®</sup> 100 SD from Roquette Frères. Tabletability was evaluated by compacting 400 mg tablets using a compaction simulator (Styl'One Evolution, Medelpharm, France) following Korsch XL-400 simulation with compaction speeds of 63,000 tablets/hour (30 rpm) and 136,500 tablets/hour (65 rpm). A flat-faced, 11.28 mm tooling set, under external lubrication with magnesium stearate was used. Drug release was evaluated with drugs of differing solubilities, namely propranolol hydrochloride (high solubility, 50 mg/mL) and metformin (very high solubility, 300 mg/mL). The controlled release performance of drug-containing co-processed HPMC-mannitol tablets was benchmarked against corresponding commercial products. Tablet shape and drug content were matched with the marketed formulations Ciplar LA 40 mg (Cipla, India) and Glucophage XR 500 mg (Merck). Dissolution studies were conducted with USP dissolution apparatus II, using a physiologically relevant, pH transition method adapted from USP <711> Dissolution Method A.

#### RESULTS

HPMC particles generally appeared elongated and striated when observed under scanning electron microscopy, while spray-dried mannitol, PEARLITOL® 100 SD comprised predominantly spherical, rough particles. Spray coating HPMC particles with mannitol solution resulted in larger, rounder particles for PEARLITOL® CR-H due to deposition of mannitol on the surfaces of HPMC particles (figure 1).



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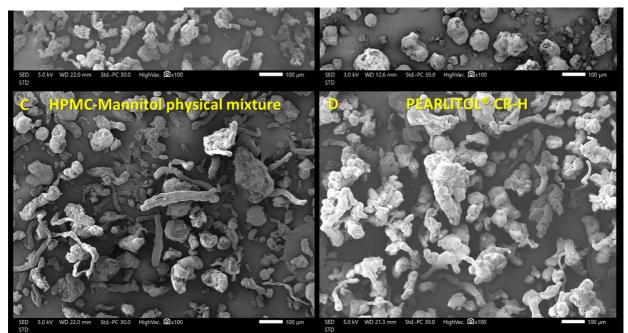


Figure 1. Scanning electron microscopy images of HPMC (A); spray-dried mannitol (B); physical mixture of HPMC and spray-dried mannitol (C); and PEARLITOL<sup>®</sup> CR-H via fluid bed spray granulation (D). Scale bars represent 100 μm.

The larger size and rounder shapes of PEARLITOL<sup>®</sup> CR-H particles was inferred to provide improved powder flowability, as characterized by angle of repose, Hausner ratio and flow time measurements (figures 2[A]) and 2[B], and tables 1 and 2). PEARLITOL<sup>®</sup> CR-Hshowed excellent flowability based on flow time (12 s/100 g powder). The starting HPMC material recorded an angle of repose of 39.2° (fair flow by USP classification) and Hausner ratio of 1.41 (poor flow by USP classification). Compared to standard HPMC, direct compression HPMC did not demonstrate improvement in angle of repose values, and only slightly better Hausner ratio values showing poor-to-passable flow. The addition of mannitol to HPMC either by blending or

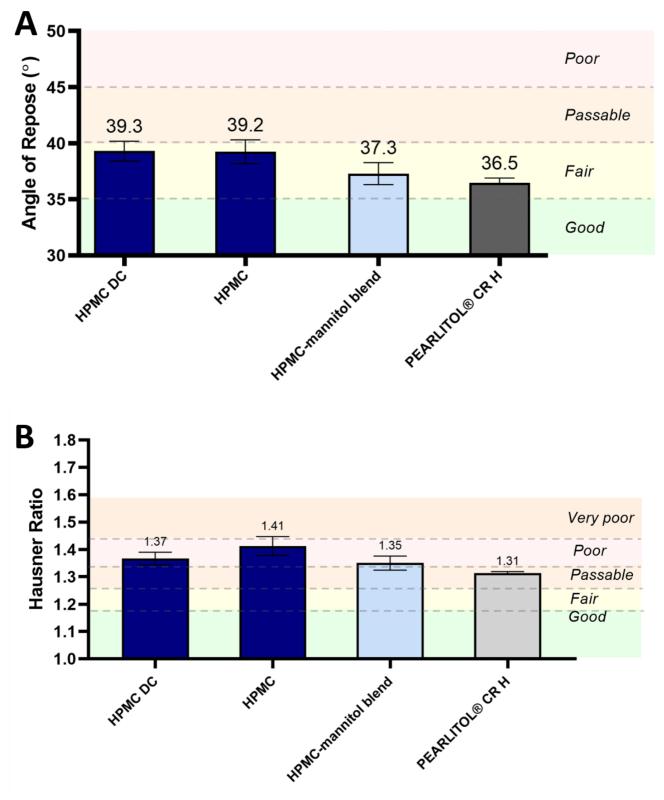


Figure 2. Flow properties of PEARLITOL<sup>®</sup> CR-H in comparison to direct compression grade HPMC (HPMC DC), pure HPMC and physical blend of HPMC-mannitol: Angle of repose (A) and Hausner ratio (B).

 Table 1. Flow properties of PEARLITOL ® CR-H batches using "flow through an orifice" following Ph. Eur. Chapter 2.9.16 – Flowability. Apparatus II was used with a 10mm orifice. 100g of powder was sampled for each measurement.

	PEARLITOL <sup>®</sup> CR-H Batch 01	PEARLITOL <sup>®</sup> CR-H Batch 02	PEARLITOL <sup>®</sup> CR-H Batch 03
Flow time (seconds/100g)	12	12	12
Bulk density (g/cm <sup>3</sup> )	0.29	0.33	0.31

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Hausner ratio	1.31	1.32	1.31
Angle of repose (°)	36	36.7	36.6

Table 2 presents flow characteristics of powder blends containing a poorly flowable powder (PEARLITOL® 50 C) standing for a poorly flowable active pharmaceutical ingredient (API). Results clearly show a significant improvement of the flowability brought by PEARLITOL® CR-H in comparison to HPMC DC grade and HPMC/mannitol DC grade (PEARLITOL® 100 SD) blend.

 Table 2. Flow properties of PEARLITOL® CR-H in comparison to HPMC DC grade and physical blend of HPMC–mannitol using orifice flow method

 (EP Chapter 2.9.16 – Flowability, Apparatus II, 10mm orifice). 100g of powder was used for each measurement. PEARLITOL® 50C (Roquette Frères,

 France) was used to model after an API with poor flow. Each formula contains 30% of this poorly flowable powder.

	PEARLITOL <sup>®</sup> CR-H + PEARLITOL <sup>®</sup> 50 C	HPMC DC grade + PEARLITOL <sup>®</sup> 50 C	Blend: 70 % HPMC DC grade / 30 % PEARLITOL® 100 SD + PEARLITOL® 50 C
Flow time (seconds/100g)	8	No flow	No flow
Bulk density (g/cm <sup>3</sup> )	0.42	0.38	0.41
Tapped density (g/cm <sup>3</sup> )	0.57	0.58	0.61
Hausner ratio	1.37	1.53	1.49
Angle of repose (°)	37	44	39

Figure 3 compares the tabletability of PEARLITOL® CR-H and the physical blend HPMC-mannitol at two simulated industrial speeds.

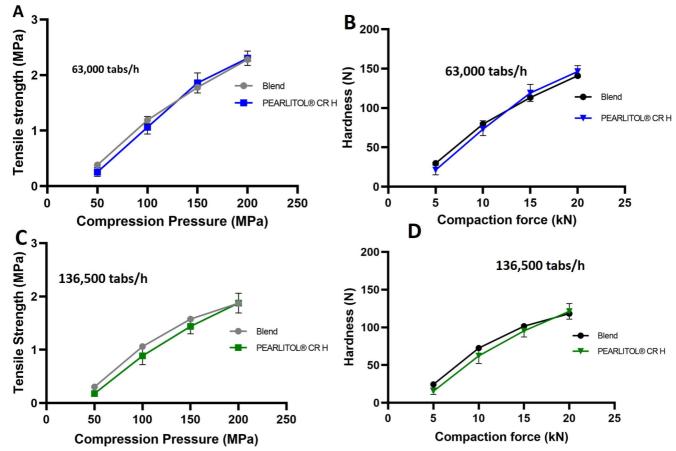


Figure 3. Tabletability of PEARLITOL® CR-H versus physical blend of HPMC–mannitol at two compression speeds of 63,000 tablets/hour – tablet tensile strength (A); hardness (B), and 136,500 tablets/hour – tablet tensile strength (C); hardness (D), following Korsch XL-400 simulation on Styl'One Evolution compaction simulator.

As shown on figure 3, both the physical mixture and co-processed HPMC-mannitol produced tablets of high tensile strength > 1.6 MPa at

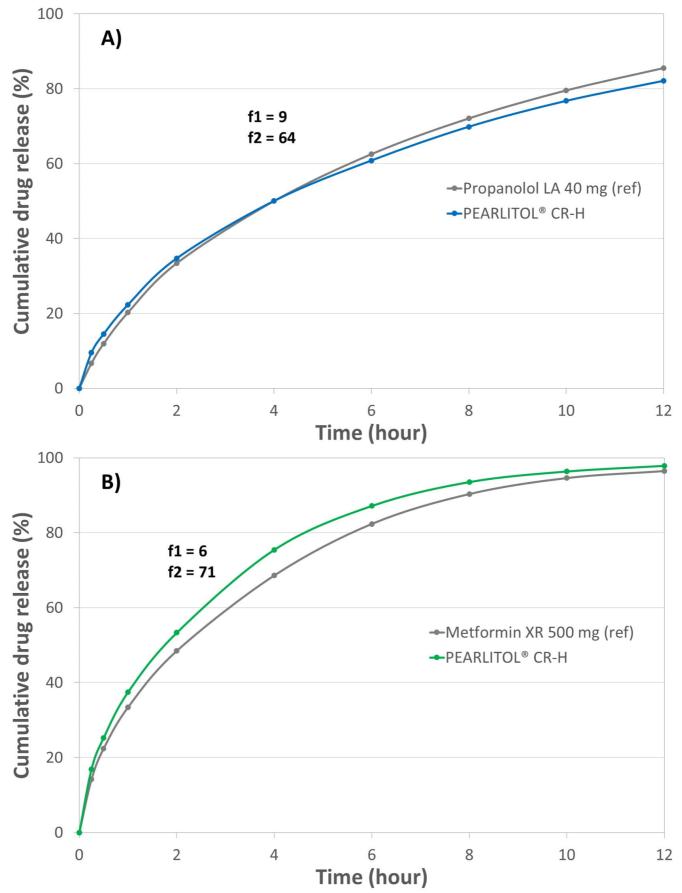


Figure 4. Drug release performance of PEARLITOL<sup>®</sup> CR-H co-processed HPMC–mannitol in comparison to commercial products for metformin HCl (A) and propranolol HCl (B). Similarity factors (f1 and f2) are embedded in the graphs.

The tablets made in-house from PEARLITOL® CR-H exhibit a similar drug release profile when compared to the commercial products for both

## CONCLUSION

PEARLITOL<sup>®</sup> CR-H is an excellent candidate for a directly compressible, controlled release excipient due to improved flowability and good tabletability. PEARLITOL<sup>®</sup> CR-H demonstrates excellent controlled release performance for drugs of differing aqueous solubilities.

### REFERENCES

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