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ORALLY DISINTEGRATING TABLETS - Novel Controlled Release Formulation for Orally Disintegrating Tablets Using Ion Exchange Resins

INTRODUCTION

Oral disintegrating tablets (ODTs) are designed to disintegrate rapidly in the mouth upon contact with saliva (= 30 seconds) and allow oral drug delivery without chewing or a need for water.1 These formulations offer increased convenience and ease of use with the potential to improve patient-dosing compliance - especially in certain patient populations (eg, pediatric, geriatric, mentally disabled, and bed-ridden patients), for which swallowing conventional solid oral dosage forms may be difficult or impossible.2 In addition to convenience and improved patient compliance, ODTs offer accurate dosing; enhanced bioavailability by greater pre-gastric drug absorption in the mouth, pharynx and esophagus, and often a better safety profile by reduced likelihood of choking or suffocation.3

The popularity of ODTs has surged in the past decade, and currently, more than 50 medicines in various cardiovascular, psychiatric, analgesics, and antihistamine indications are available as ODT formulations.3,4 Further, marketing studies have shown that greater than 50% of patients prefer ODTs compared with other solid dosage forms, and roughly 70% purchase ODTs, even though liquid and tablet formulations of a drug are also commercially available.5 This may, in part, be attributed to known ODT advantages that include portability, convenience, ease of swallowing, and a pleasant taste that often masks the bitterness of most orally bioavailable active pharmaceutical ingredients (APIs).

PROPERTIES OF ODTS

Not every medication is amenable for ODT formulation. Ideally, ODT formulations should not require water to swallow and will dissolve or disintegrate in the mouth. These formulations should allow high API (drug) loading, be compatible with tastemasking and other excipients, have a pleasing mouth feel, leave little or no residue in the mouth after administration, possess sufficient strength and physical properties to withstand

BIOGRAPHIES



Dr. Abhijit Gokhale is a Senior Scientist (Formulations and Process Development) employed at Patheon Pharmaceuticals since May 2011. Dr. Gokhale has over 12 years of drug development experience in both academic and industrial environments. He has extensive experience in formulating pharmaceutical drugs for both controlled release as well as bioavailability improvement applications. Dr. Gokhale has authored several papers and patents in the field of nanoparticle-based drug delivery and several cutting-edge technologies used in formulations. pharmaceutical manufacturing and packaging processes, and exhibit low sensitivity to environmental factors such as temperature and humidity.

Drugs that are typically not amenable to ODT formulations include those that present tastemasking difficulties or that require controlled or sustained release.3-6 However, as the demand for ODTs continues to grow, formulation scientists are exploring ways to adapt ODT formulations for drugs that require controlled or sustained release for optimal therapeutic benefits.

ION EXCHANGE RESINS IN ODT FORMULATIONS

Ion exchange resins (IERs) are water-insoluble cross-linked polymers containing a salt-forming group at repeating positions on the polymer chain.7 Synthetic IERs are usually cast as porous beads with considerable external and internal pore surfaces for loading. The resins are typically spherical in shape and 0.5 to 1.0 mm in diameter. The structure of these IERs is quite porous at a molecular scale to achieve the drug loading.

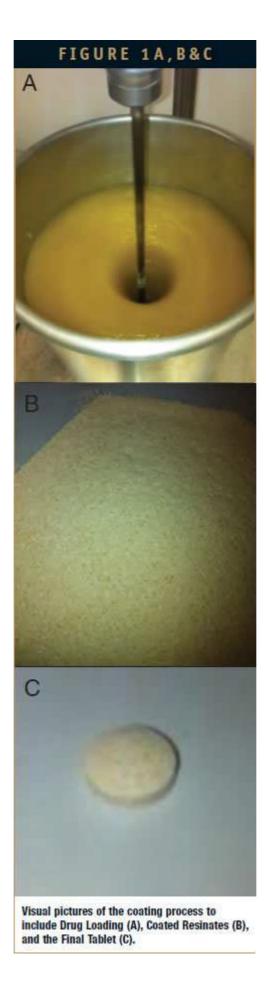
IERs are broadly classified into two main categories: cation exchange resins and anion exchange resins, which have the



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ability to exchange counter-ions within aqueous solutions surrounding them.7 Cation exchange resins contain either strong acidic groups (eg, sulfonic acid groups) or weak acidic groups (eg, quaternary amino groups). Anion exchange resins contain either strong basic groups (eg, carboxylic groups) or weak basic groups (eg, amino groups).

Selection of an appropriate IER is largely dependent upon the exchangeable ion properties of a specific drug. When choosing an IER for the sustained-release application, two main factors must be considered: cross-linking properties and drug loading capacity.7,8 The typical range of cross-linking is 4% to 16%. For drug loading considerations, the resin acid/base strength and counter-ion selectivity are important.7,8



Drugs are loaded onto the resins via an exchange reaction, forming drug-resin complexes called resinates. Insoluble resinates are formed through weak ionic bonding with oppositely charged drugs so that release of a drug from a resinate

does not occur at salivary pH (~ 6.7).7-9 The resins are not absorbed by the body due to their high molecular weight and water insolubility and are therefore inert; making them ideal drug delivery vehicles. To that end, ion exchange resins are used for a variety of applications in the pharmaceutical industry, such as:8,10

- Taste-masking
- Disintegrant /Superdisintegrant
- Solubility improvement
- Drug stabilization
- · Improved flow rates
- Modified-/Sustained-release profiles
- Therapeutics

Junyaprasert et al formulated sustained-released suspensions of diltiazem (a short half-life calcium channel blocker) using strong cation exchange resins.11 Likewise, Steel et al studied a novel combination vector consisting of the adenovirus conjugated to liposomes bound to cation-exchanging microspheres as a sustained release gene therapy delivery vehicle.12 Jeong et al investigated the complex formation between drugs and cation exchange resins and the effects of coating by various aqueous polymeric dispersions on the complexes to develop new sustained release ODTs of the cough suppressant dextromethorphan.13,14 All these aforementioned studies show the successful sustained release of drug molecules using IER technique.

Ingredients	Formulation A	Formulation B
Drug Loaded Resins		
Model Drug	10.3%	10.3%
Amberlite [™] IRP69	41.1%	20.5%
Functional Coating Eudragit® RS	3.3%	2.0%
Eudragit [®] RL	1.4%	0.9%
Triethyl Citrate	0.5%	0.3%
Talc	2.4%	1.4%
Tablet Ingredients		
Mannitol	27.9%	43.9%
Ac-di-Sol®	4.1%	6.5%
Citric Acid	4.1%	6.5%
Sodium Bicarbonate	4.1%	6.5%
Mg Stearate	0.8%	1.2%
Total	100.0%	100.0%

EXPERIMENTAL METHOD & MATERIALS

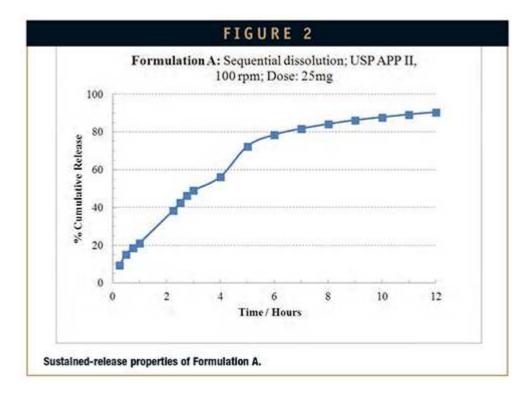
In the present study, a strong cation exchange resin, AmberliteTM IRP69, was used to form IER-drug resinates. Amberlite IRP69 was considered to be suitable for the model drug compound based on the drug properties. The model drug used in this study was a very bittertasting HCL salt, making it difficult to formulate in ODT formulations.

The Amberlite IRP69-drug resinates were created by mixing hydrated ionexchange resin particles and different concentrations of the model drug substance. Mixtures were stirred for 6 hours to maximize drug loading onto the IER particles. The samples were taken at 1, 2, 4, and 6 hours to investigate the drug loading. The drug loaded resins were then dried in an oven and coated with a combination of methacrylate polymers to further control the release profile by reducing the initial burst. Figure 1 shows the manufacturing process.

Formulations were developed by varying the material composition and optimizing the process parameters. Croscarmellose Sodium (Ac-di-Sol®) was used as a superdisintegrant to obtain tablet disintegration within 15 seconds. Mannitol, citric acid, and sodium bicarbonate helped to mask the taste of the bitter drug compound as well as to enhance the disintegration time along with Ac-di-Sol. Table 1 provides the details of the two formulations. The blend was then compressed using 11/32" round tooling into 250-mg tablets. Both formulations have a dose of 25 mg. The physical properties of both of the formulations are presented in Table 2.

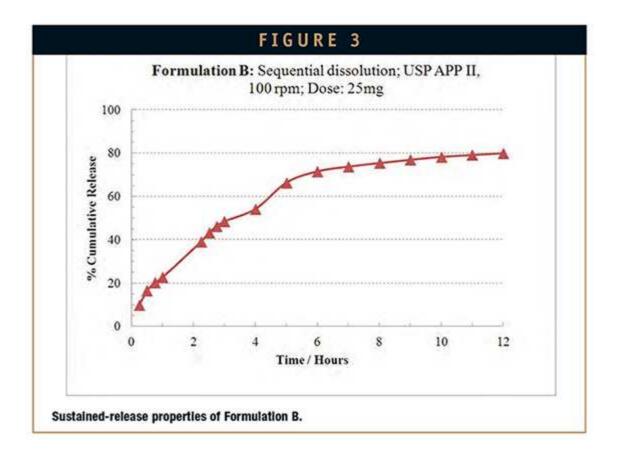
RESULTS & DISCUSSION

Both formulations were tested in standard sequential dissolution (2 hours in pH 1.2 buffer followed by 10 hours in pH 6.8 buffer) to investigate the release characteristics. Figures 2 and 3 show the dissolution profiles of the formulations. Both formulations exhibit sustained drugrelease characteristics. The comparison of the dissolution profiles is demonstrated in Figure 4.



Both formulations presented in the study had a tablet hardness of 15 KP and were identical in all aspects except the ratio of Amberlite IRP69 to drug substance. The amount of Amberlite IRP69 in the formulations varied, and the tablet weight was maintained by adjusting mannitol quantity to obtain the dose similar formulations. The dissolution profiles of both of the formulations showed that the drug release is independent of the concentration and exhibits Fickian characteristics. Each of the formulations disintegrated in less than 15 seconds, demonstrating the ODT nature of the tablets.

The friability of both of the formulations was 0.02%. The flowability of the granules was acceptable for both of the formulations and no undesired bridging, rat holes, or sticking to the tooling were observed during compression.



	Formulation A	Formulation B
Tablet Disintegration	<15 seconds	<15 seconds
Tablet Hardness	15 KP (<u>+</u> 1KP)	15 KP (<u>+</u> 1KP)
Tablet Shape	11/32" Round	11/32" Round
Tablet Friability	0.02%	0.02%

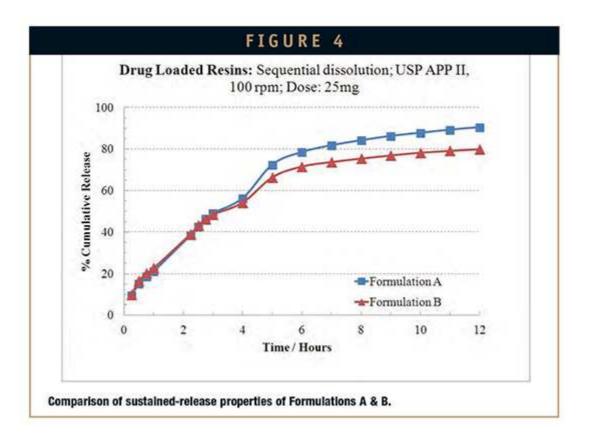
CONCLUDING REMARKS

The drug formulation technique described in this article is simple and easily scalable. Because of the availability of a wide range of anionic and cationic IERs, a vast array of pharmaceutical drugs can be formulated using this technique to achieve sustained release of drug molecules.15 In addition, IERs can be used as taste-masking agents and superdisintegrants in ODT formulations.

Combining the taste-masking and sustained-release characteristics of IERs to formulate ODTs will help to improve drug dosing compliance among pediatric, geriatric, bedridden, and non-cooperative patients.16,17 Moreover, the popularity of ODTs amongst members of the general population is likely to increase because of their portability, ease of use, and convenience.

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